

Heterogeneous Tumor Microenvironment in Non-Small Cell Lung Cancer derived from FDG-PET Data

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1. Introduction

- FDG-PET provides voxel-wise Standard Uptake Value (SUV)
- Standard use: scalar biomarker (metabolic activity)
- **Goal:** Recover underlying tumor properties from SUV
- **Key idea:** Combining:
 - Biophysical porous-media model
 - Transport + reaction of tracer (FDG)
 - Ensemble smoother - multiple data assimilation (ES-MDA)

2. Physical Model

Tumor modeled as a two-phase porous medium with cancer cells (α_c) and interstitial fluid (α_w) and extracellular matrix (ECM) as solid phase

Key processes:

- Fluid flow (Darcy-type):

$$\begin{aligned} (\alpha_c)_t + \nabla \cdot (\alpha_c \mathbf{u}_c) &= 0 \\ (\alpha_w)_t + \nabla \cdot (\alpha_w \mathbf{u}_w) &= Q, \quad Q = Q_v - Q_l \\ \alpha_c \nabla P_c &= -\zeta_c \mathbf{u}_c + \zeta_{cw} (\mathbf{u}_w - \mathbf{u}_c) \\ \alpha_w \nabla P_w &= -\zeta_w \mathbf{u}_w - \zeta_{cw} (\mathbf{u}_w - \mathbf{u}_c) \end{aligned}$$

$$\begin{aligned} \alpha_c + \alpha_w &= 1 \\ P_c &= P_w + \Delta P(\alpha_c) + \Lambda(C) \\ Q_v &= T_v(x) (P_v^* - P_w) \\ Q_l &= T_l(x) (P_w - P_l^*) \end{aligned}$$

- In addition to equations above there are chemical agents influencing tumor progression

- Advection-diffusion of FDG
- Delivery of FDG to interstitial space

$$\begin{aligned} d_t + \nabla \cdot (\mathbf{u}_w d) &= \nabla \cdot (D_d \nabla d) + \varepsilon_{\text{vasc}}^c Q_v d_v^* \\ &+ \varepsilon_{\text{vasc}}^d P^* T_v (d_v^* - d) - \lambda_c (\alpha_c d - \delta_d^c d^c) \end{aligned}$$

- Uptake of FDG by cancer cells ($d^c(x, t)$):

$$\frac{d}{dt} d^c(x, t) = \lambda_c (\alpha_c d - \delta_d^c d^c).$$

- SUV represents final uptake/trapping by cancer cells relatively total injected dose
- FDG is injected and images are acquired approximately 60 min post injection

3. Inverse Problem

- We tune the spatial varying fields $\alpha_c^0(x)$, $T_v(x)$, $T_l(x)$ and the parameters $\varepsilon_{\text{vasc}}^d \in [0.1, 1]$, $\varepsilon_{\text{vasc}}^c \in [0, 0.25]$ and $\delta_d \in [0.05, 0.25]$
- Due to lack of information we solve the estimation problem for $\lambda_c = \{0.05, 0.15, 0.30\}$ (low, intermediate and high uptake of FDG) and $k_w = \{1, 4, 16\}$ (low, intermediate, high density of tumor tissue)

4. Data assimilation

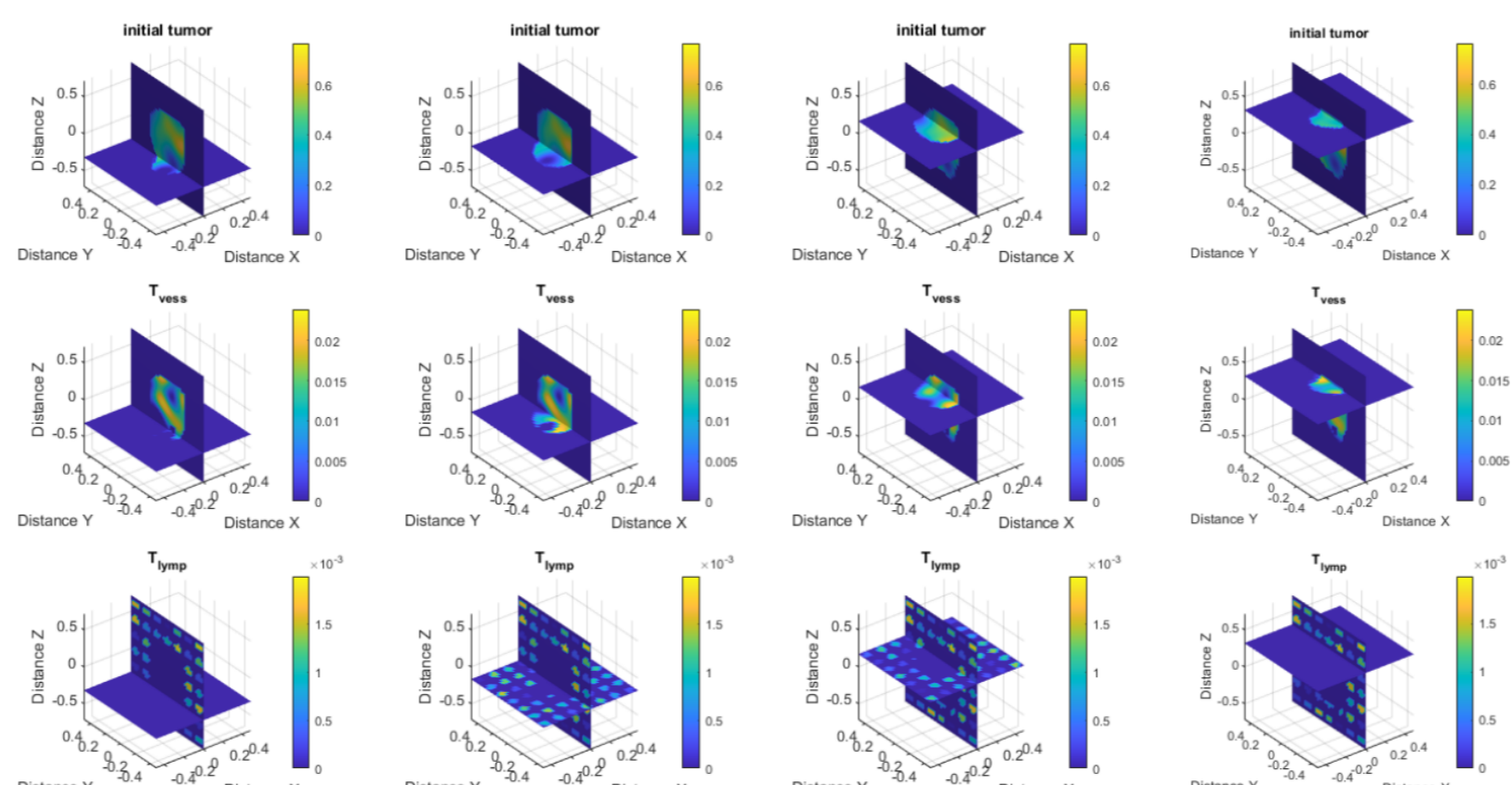
- Y : observed SUV (3D field)
- $V = [\alpha_c^0(x), T_v(x), T_l(x), \varepsilon_{\text{vasc}}^d, \varepsilon_{\text{vasc}}^c, \delta_d]$: parameter vector
- G : nonlinear forward model
- Cost function

$$J(V) = \frac{1}{2} (Y - G(V))^T \Gamma^{-1} (Y - G(V))$$

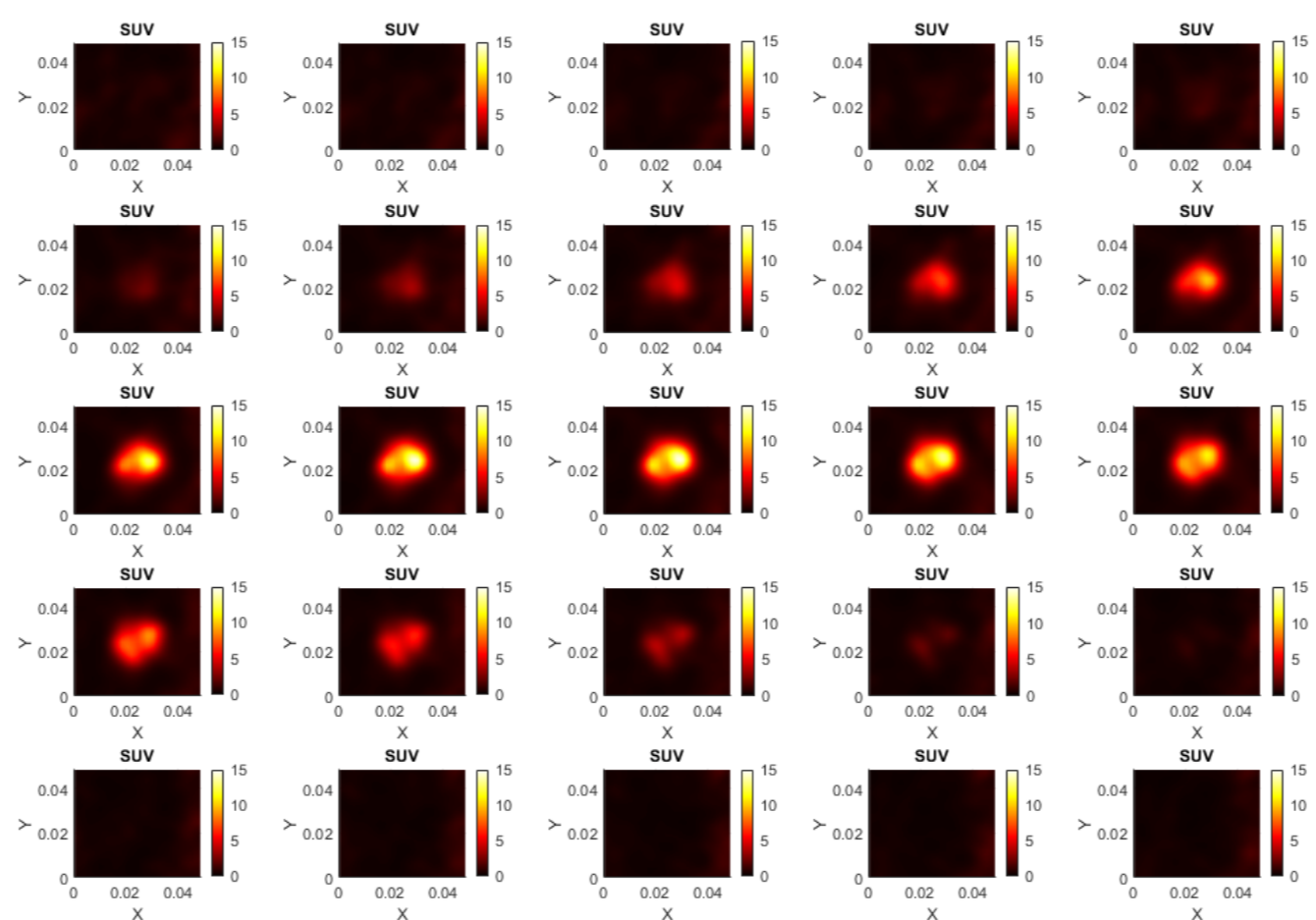
is minimized using ES-MDA with 4 iterations

Prior distribution:

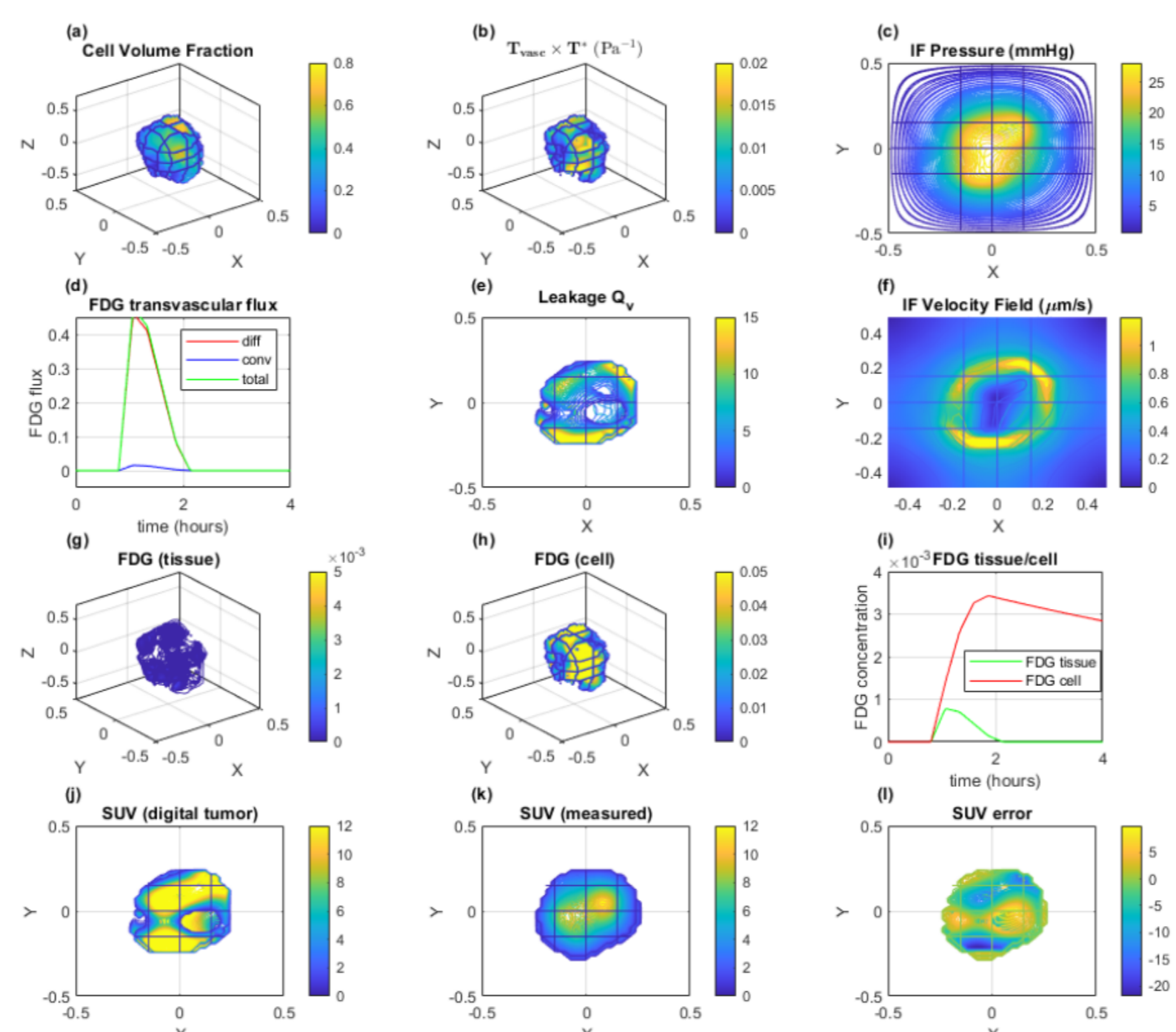
- $\alpha_c^0(x)$ generated using Gaussian variogram
- $T_v(x)$ generated using Gaussian variogram and multiplied by a random factor
- $T_l(x) = T_{l,k} J_k(x)$ where $J_k(x)$ are uniformly distributed "balls" in peritumoral region and $T_{l,k}$ are uniformly distributed
- $\varepsilon_{\text{vasc}}^d$, $\varepsilon_{\text{vasc}}^c$ and δ_d are uniformly distributed



Initial ensemble member



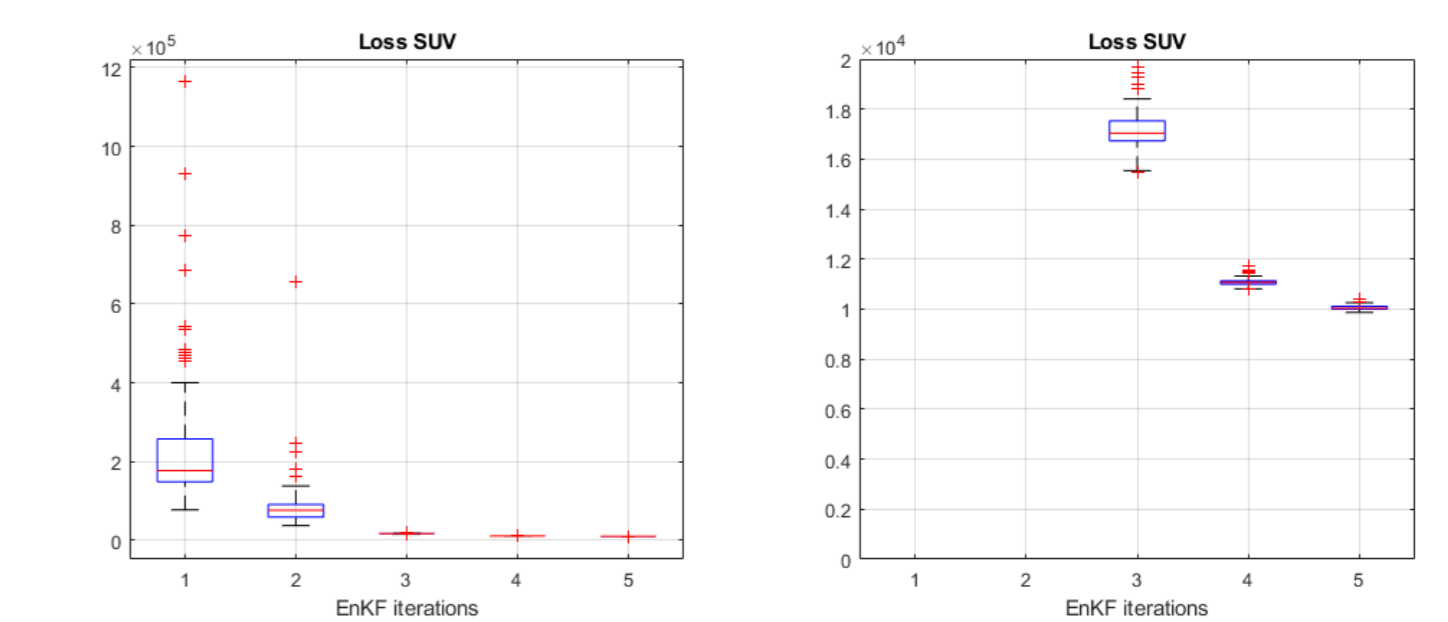
SUV data from patient



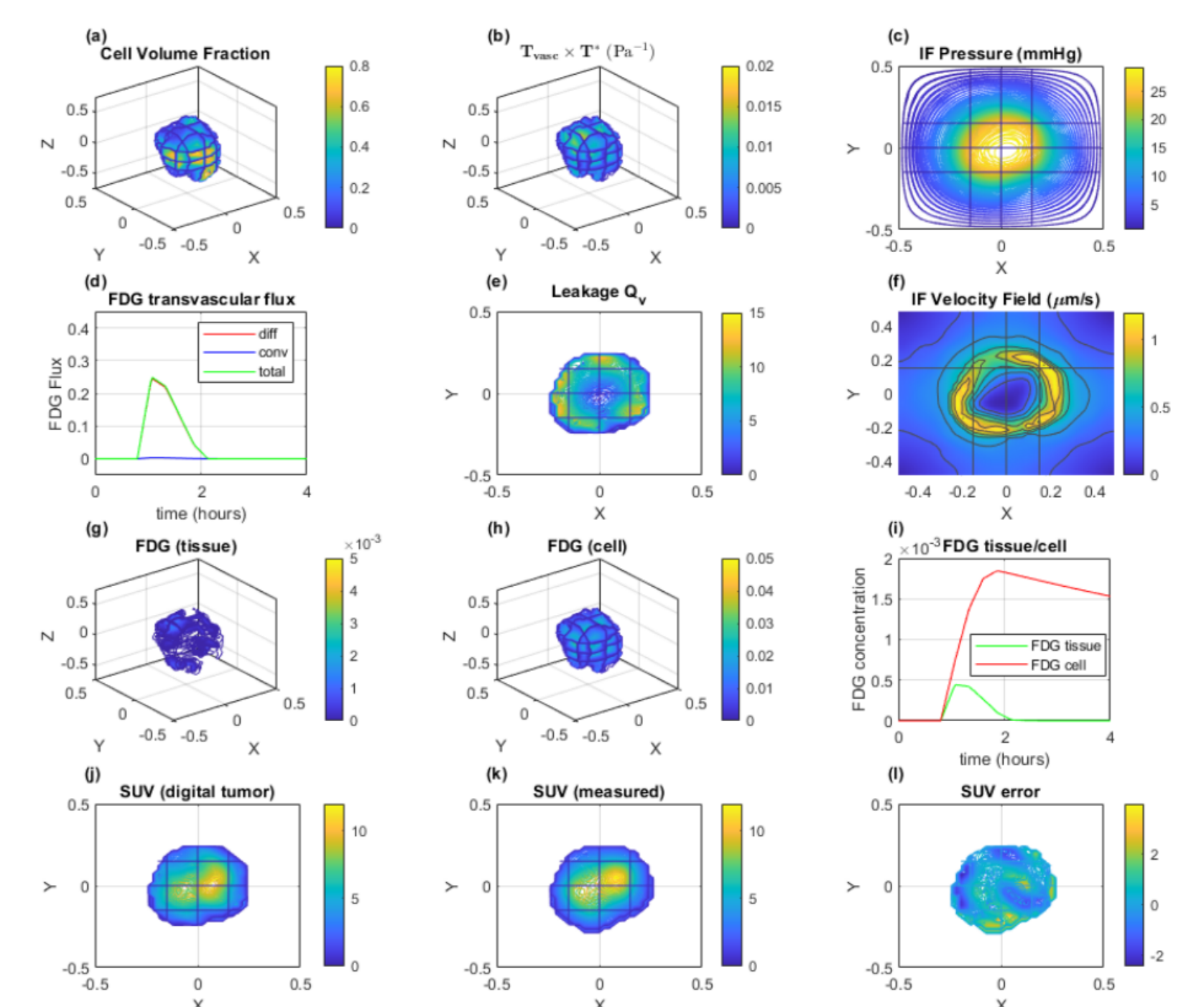
Simulation with an initial ensemble member with $\lambda_c = 0.30$ and $k_w = 1$

5. Results from data assimilation

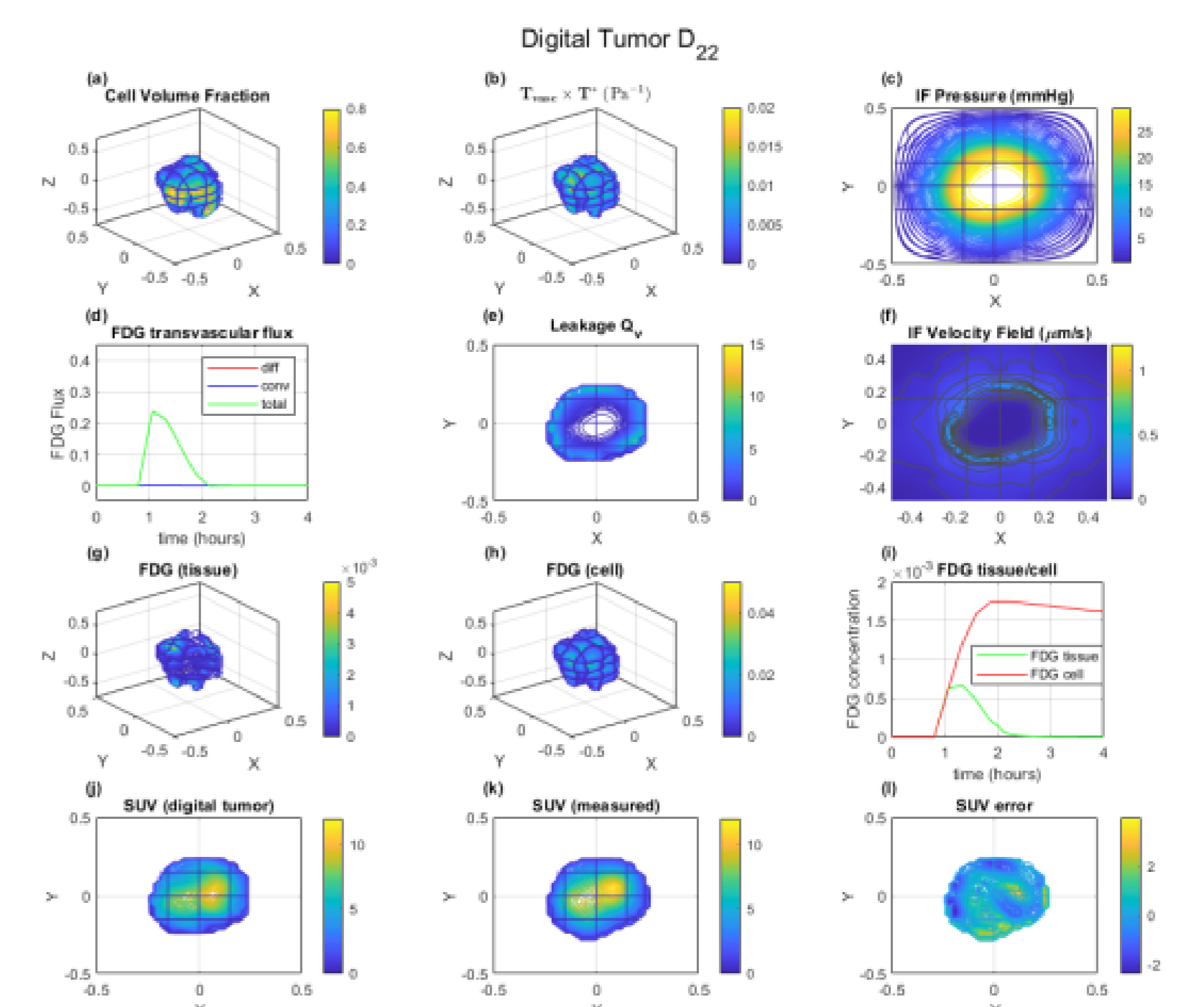
- EnKF reduces mismatch between simulated and observed SUV
- Spatial patterns reproduced after few iterations



Loss function per iteration for the case with $\lambda_c = 0.30$ and $k_w = 1$



Simulation with final ensemble mean with $\lambda_c = 0.30$ and $k_w = 1$



Simulation with final ensemble mean with $\lambda_c = 0.15$ and $k_w = 4$

- Find solutions matching data for all 9 combinations of parameters λ_c and k_w

6. Conclusions

- Find parameter vectors that reproduce SUV data
- Not able to resolve ambiguity with respect to λ_c and k_w
- Complementary information/data?
- Promising framework for further investigations



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